

Design and fabrication of a planar patch-clamp substrate using a silicon-on-insulator wafer

Zhang Zhenlong(张振龙), Liu Xiangyang(刘向阳), and Mao Yanli(毛艳丽)[†]

(Institute of Optics and Photoelectronic Technology, School of Physics and Electronics, Henan University, Kaifeng 475004, China)

Abstract: The planar patch-clamp technique has been applied to high throughput screening in drug discovery. The key feature of this technique is the fabrication of a planar patch-clamp substrate using appropriate materials. In this study, a planar patch-clamp substrate was designed and fabricated using a silicon-on-insulator (SOI) wafer. The access resistance and capacitance of SOI-based planar patch-clamp substrates are smaller than those of bulk silicon-based planar substrates, which will reduce the distributed RC noise.

Key words: planar patch-clamp substrate; silicon-on-insulator; access resistance; capacitance

DOI: 10.1088/1674-4926/30/9/096001

PACC: 0710C; 8780B

1. Introduction

Ion channels are transmembrane pores which allow the passage of ions into and out of a cell down the electrochemical gradient, which play key roles in many cellular processes^[1,2]. There are many distinct dysfunctions known as channelopathies caused by ion channel mutations^[3]. Therefore the investigation of ion channels is of great significance for understanding how they work and for drug discovery of channelopathies.

The pipette patch-clamp technique has proven to be a powerful technique for the investigation of fundamental ion channel biophysics and for drug discovery^[4,5]. This technique allows one to monitor the gating of ion channels under defined conditions and enables the coupling of functional and molecular studies on ion channels at the single cell level^[6]. However, this technique has some weaknesses, such as the requirement of precise micromanipulation and a skilful experimenter, and the fact that the electrode is an individual glass pipette, which are not suitable for application to high-throughput screening^[7,8]. Recently a planar patch-clamp method has attracted increasing attention, because it has some advantages compared with the pipette patch-clamp method, such as the miniaturization and parallelization of the planar substrates and the ability to combine with other physical probes^[9,10].

Many materials have been used for planar patch-clamp substrate fabrication, such as glass^[11], Si^[12-14], quartz^[15] and PDMS^[16]. It has been considered for Si that the background noise current is large due to the high density of free charge carriers in the substrate. However, we have recently demonstrated that the noise current can be significantly reduced by using a silicon-on-insulator (SOI) substrate^[17]. There are several other advantages to using an SOI substrate: (1) the structure of the micropore through the substrate can be precisely controlled by using the large etching rate difference between Si and SiO₂ in

both plasma and wet etching, and (2) it is possible to produce significantly miniaturized devices by integrating the biosensor and Si electronic circuits of the preamplifier into the same SOI substrate.

In this study, we design and fabricate a planar patch-clamp substrate using an SOI wafer. The access resistance and capacitance of the SOI-based planar patch-clamp substrate are smaller than those made with a bulk silicon wafer due to the special structure of the SOI wafer. Therefore the noise current in the experiments must be smaller because the small access resistance and capacitance induce small current noise^[18].

2. Experimental

An N-type SOI substrate (50–75 Ω -cm resistivity with about 600 μ m total thickness) with 2.5 μ m top Si layer and 3 μ m buried SiO₂ layer was cut to a square of size 7 \times 7 mm² after the formation of the micropore. The backside thick Si layer was etched by 8% tetramethylammonium hydroxide (TMAH, Wako), and the buried SiO₂ layer was etched by 10% solution of HF (Steller Chemifa, Japan).

The intracellular solution in the cell experiments contains (in mM): 140 KCl, 5 EGTA, 10 HEPES, pH 7.4 (with KOH). The extracellular solution contains (in mM): 140 NaCl, 5 KCl, 2 MgCl₂, 2 CaCl₂, 10 Glucose, 10 HEPES, pH 7.4 (with NaOH). All the chemicals were purchased from Sigma-Aldrich, of analytical grade, and used without further purification. Water with a typical resistivity of 18.2 M Ω -cm was produced with Milli-Q purification (Millipore Ltd.).

The access resistance and capacitance of the substrate were measured with an Axopatch 200B Amplifier (Axon Instruments) and a Digidata 1322A interface (Axon Instruments) connected to a computer. The results were acquired using the pClamp 9.0 program (Axon) at 500 Hz.

[†] Corresponding author. Email: myl3000@163.com

Received 1 March 2009, revised manuscript received 1 April 2009

© 2009 Chinese Institute of Electronics

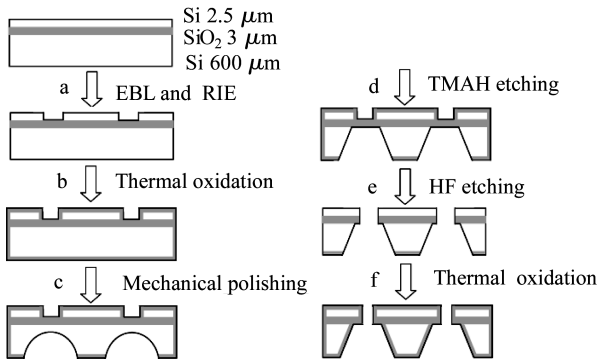


Fig. 1. Procedures of SOI-based planar patch-clamp substrate fabrication using EBL and RIE.

3. Results and discussion

3.1. Design and fabrication of the planar patch-clamp substrate

Figure 1 shows the through-pore fabrication procedures in an SOI wafer using electron beam lithography (EBL) and reactive ion etching (RIE). Firstly circular patterns were made in the substrate with the EBL and RIE techniques (Fig. 1(a)). Then a SiO₂ layer of 1 μm thickness was grown at 900 °C with thermal oxidation in which O₂ bubbled water vapor at 95 °C was used as the reactive gas (Fig. 1(b)). This thermally formed SiO₂ layer is for protecting the top surface of the substrate in the subsequent tetramethylammonium hydroxide (TMAH) etching process. Then large holes were made by 1 mm diameter diamond drill polishing the backside of the substrate (Fig. 1(c)), followed by 8% (v/v) TMAH etching at 90 °C to the buried SiO₂ layer (Fig. 1(d)). Finally the buried SiO₂ layer at the bottom of the pattern was removed with 10% (v/v) HF solution from the topside of the substrate (Fig. 1(e)), followed by 1 μm thick SiO₂ layer formation at 900 °C with thermal oxidation in the presence of O₂ bubbled water vapor at 95 °C (Fig. 1(f)). This thermal SiO₂ layer is for decreasing the capacitance of the substrate and reducing the pore diameter. Figure 2 shows the SEM images of a single pore and the schematic of the pore wall after the processes a, b, e and f shown in Fig. 1, respectively. From the SEM of the substrate, the final diameter of the pore is about 1 μm. In the present study, substrates with diameters of 1–2 μm were fabricated, which were demonstrated to be suitable for high seal resistance formation and ion-channel current measurement^[11, 15, 16].

3.2. Electrical properties of the SOI-based planar patch-clamp substrate

Ion channel current recording needs sufficient signal intensity compared with the background noise. In the pipette patch-clamp experiment, the background noise is generated from many sources, such as the amplifier, cell membrane, glass-membrane seal, pipette, pipette holder and interactions between all of them^[5]. In the planar patch-clamp experiment, the microstructured substrate replaces the pipette holder and glass pipette in the pipette patch-clamp experiment. From the

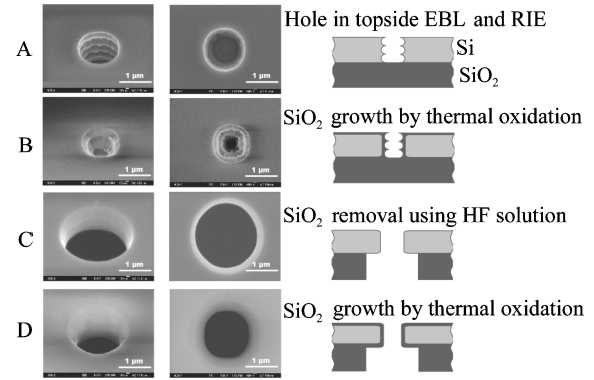


Fig. 2. SEM images of a single pore and the schematic of the pore wall after the processes a, b, e and f shown in Fig. 1, respectively. SEM images in the left and middle panels are the oblique view and top view of the same pore. The light-gray and dark-gray layers in the illustrations represent Si and SiO₂, respectively.

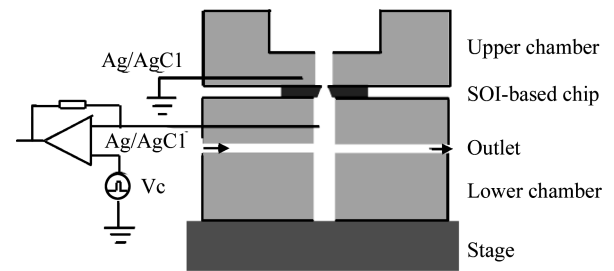


Fig. 3. Setup for the measurement of access resistance and capacitance of the substrate.

viewpoint of reducing the background noise, it is required that the access resistance and the capacitance of the fabricated substrate be small, because small access resistance and capacitance produce small distributed RC noise^[18].

The access resistance of the planar substrate is dominated by the conductance of the electrolyte in the pore because the area of the pore is very small compared with the rest of the conducting path^[13]. Therefore the access resistance can be evaluated by only taking into account the resistance of the solution in the pore, which is given by

$$R_a = \frac{\rho l_p}{A} \quad (1)$$

with access resistance R_a , resistivity of the solution ρ , cross-sectional area of the pore A , and length of the pore l_p .

The access resistance and capacitance of the substrate were measured with the setup shown in Fig. 3. The SOI-based substrate was sandwiched between the upper chamber and the lower chamber. The Ag/AgCl electrodes were inserted in the upper and lower chambers. In our experiments, the diameter of the pore is between 1 and 2 μm, and the access resistance was measured to be 0.5–2.3 MΩ with bath solution in the upper chamber and pipette solution in the lower chamber. Figure 4 shows the variation of the access resistance with pore diameter.

The capacitance of the substrate can be evaluated by

$$C = \left(\frac{1}{C_1} + \frac{1}{C_2} + \frac{1}{C_3} + \frac{1}{C_4} + \frac{1}{C_5} \right)^{-1}, \quad (2)$$

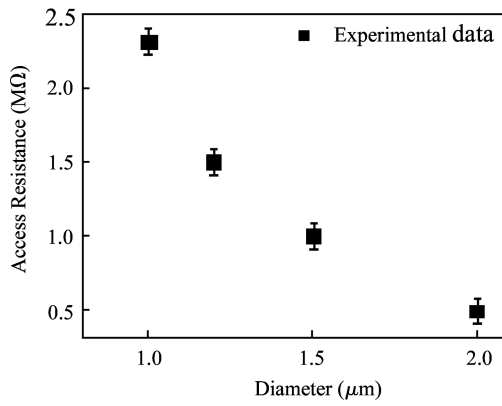


Fig. 4. Variation of access resistance with pore diameter.

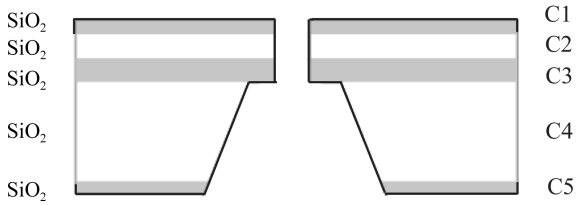
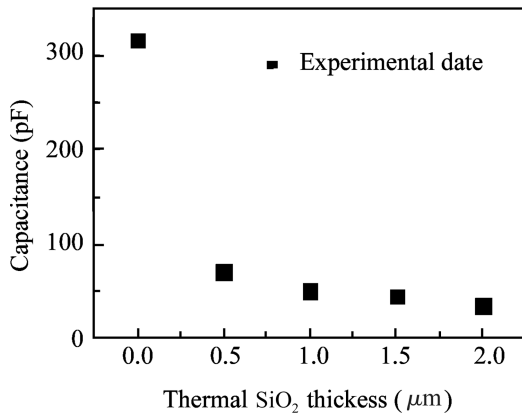


Fig. 5. Schematic cross section of the SOI-based substrate.

Fig. 6. Variation of substrate capacitance with thermal SiO₂ layer thickness.

$$C_i = \epsilon_0 \epsilon_r \frac{S_i}{d_i}, \quad (3)$$

where C stands for the total capacitance of the substrate, C_i for the capacitance of the SiO₂ or silicon layer (Fig. 5), ϵ_0 for the dielectric constant of free space, ϵ_r for the relative dielectric constant of dielectric material, S_i for the fluid contact area, and d_i for the thickness of the material. The capacitance of the substrate can be decreased by increasing the thickness of the SiO₂ layer due to the smaller relative dielectric constant. Figure 6 shows the variation of the substrate capacitance with the thermal SiO₂ layer thickness. The capacitance with the value of 35 pF was obtained with the formation of the 2 μm SiO₂ layer.

3.3. Discussion

It has been considered that the silicon wafer induces a large capacitance due to the high density of free charge carriers in silicon^[10]. This large capacitance is the main disadvantage to making a planar patch-clamp substrate because the current

Table 1. Comparison of the SOI-based and bulk silicon-based substrates.

Parameter	SOI-based substrate (ϕ 1–2 μm)	Bulk silicon-based substrate (ϕ 1–2 μm)
Access resistance (MΩ)	0.5–2.3	3–10 ^[13,14]
Capacitance (pF)	Minimum: 35	Minimum: 50 ^[19]

noise increases with capacitance^[18]. Table 1 shows a comparison of the SOI-based and bulk silicon-based substrates. The capacitance of the SOI-based substrate fabricated with 35 pF in this study was obtained by the formation of a 2 μm thick thermal SiO₂ layer. This value is less than those reported in the literature for bulk silicon-based substrates such as 54 pF^[12] and 50 pF^[19]. It is expected that the capacitance of the SOI substrate could be decreased by reducing the fluidic contact area using a microfluidic system, and/or increasing the thickness of the buried SiO₂ layer. For example, the thickness of the buried SiO₂ could be increased to 10 μm from 2.5 μm used in this study. It is more difficult to obtain such a thick SiO₂ layer for a bulk silicon wafer. Moreover, in order to reduce the capacitance, thermal oxidation or plasma-enhanced chemical vapor deposition (PECVD) was adopted to form the SiO₂ layer on the substrate after the pore was formed^[12–14], which changed the shape of the pore^[13] or the roughness of the substrate surface^[12]. In the case of the SOI substrate, the thickness of the buried SiO₂ layer and the thermal layer could be decided before making the pore with FIB, thus the original surface condition and the pore shape could remain.

Another important parameter of the substrate is the access resistance, because smaller access resistance produces smaller current noise^[18]. The thickness of the layer containing the pore could be precisely controlled to be about 5.5 μm in this study because TMAH etching stops at the buried SiO₂ layer of the SOI wafer, therefore the access resistances of the substrates are small and distribute in a narrow range (shown in Table 1). For bulk silicon wafer, the thickness of the layer containing the pore was carefully controlled to be 20–40 μm; thus the access resistances of the substrates were large and distributed in a wide range^[13,14].

4. Conclusion

In this work, a planar patch-clamp substrate was designed and fabricated using an SOI wafer, and the access resistance and capacitance were measured. The values of the access resistance and capacitance are smaller compared with the reported values of a bulk silicon-based substrate due to the special structure of SOI. It is asserted that this reduces the current noise in the measurement of ion channel current.

References

- [1] Purves D, Augustine G J, Fitzpatrick D, et al. Neuroscience. Sunderland: Sinauer Associates Inc, 2001

- [2] Hille B. Ion channels of excitable membranes. Sunderland: Sinauer Associates Inc, 2001
- [3] Kass R S. The channelopathies: novel insights into molecular and genetic mechanisms of human disease. *J Clin Invest*, 2005, 115: 1986
- [4] Neher E, Sakmann B. Single-channel currents recorded from membrane of denervated frog muscle fibres. *Nature*, 1976, 260: 799
- [5] Sakmann B, Neher E. Single channel recording. New York: Plenum, 1995
- [6] Monyer H, Lambolez B. Molecular biology and physiology at the single-cell level. *Curr Opin Neurobiol*, 1995, 5: 382
- [7] Kathryn G, Klemic J F, Sigworth F J. An air-molding technique for fabricating PDMS planar patch-clamp electrodes. *Pflugers Arch–Eur J Physiol*, 2005, 449: 564
- [8] Fertig N, Klau M, George M, et al. Activity of single ion channel proteins detected with a planar microstructure. *Appl Phys Lett*, 2002, 81: 4865
- [9] Xu J, Wang X, Ensign B, et al. Ion-channel assay technologies: quo vadis. *Drug Discovery Today*, 2001, 6: 1278
- [10] Fertig N, George M, Klau M, et al. Microstructured apertures in planar glass substrates for ion channel research. *Recept Channels*, 2003, 9: 29
- [11] Fertig N, Blick R H, Behrends J C. Whole cell patch clamp recording performed on a planar glass chip. *Biophys J*, 2002, 82: 3056
- [12] Sordel T, Raveaud S G, Sauter F, et al. Hourglass SiO₂ coating increases the performance of planar patch-clamp. *J Biotechnol*, 2006, 125: 142
- [13] Matthews B, Judy J W. Design and fabrication of a micromachined planar patch-clamp substrate with integrated microfluidics for single-cell measurements. *J Microelectromechan Syst*, 2006, 15: 214
- [14] Pantoja R, Nagaraj J M, Starace D M, et al. Silicon chip-based patch-clamp electrodes integrated with PDMS microfluidics. *Biosens Bioelectron*, 2004, 20: 509
- [15] Sett A, Burkhardt C, Weber U, et al. CYTOCENTERING: a novel technique enabling automated cell-by-cell patch clamping with CYTOPATCH chip. *Recept Channels*, 2003, 9: 59
- [16] Li X H, Klemic K G, Reed M A, et al. Microfluidic system for planar electrode arrays. *Nano Lett*, 2006, 6: 815
- [17] Uno H, Zhang Z L, Suzui M, et al. Noise analysis of Si-based planar-type ion-channel biosensors. *Jpn J Appl Phys*, 2006, 45: L1334
- [18] Wonderlin W F, Finkel A, French R J. Optimizing planar lipid bilayer single-channel recordings for high resolution with rapid voltage steps. *Biophys J*, 1990, 58: 289
- [19] Schroeder K, Neagle B, Trezise D J, et al. IonworksTM HT: a new high-throughput electrophysiology measurement platform. *J Biomol Screen*, 2003, 8: 50